Australia's National Science Agency

CorticalFlow: A Diffeomorphic Mesh Transformer for Cortical Surface Reconstruction

Leo Lebrat, Rodrigo Santa Cruz, Frederic de Gournay, Darren Fu, Pierrick Bourgeat, Jurgen Fripp, Clinton Fookes, and Olivier Salvado











Regular Surface Reconstruction From Volumetric Images





Cortical Surface Reconstruction From MRI (CSR)

"The diagnosis, prognosis, and study of neurodegenerative diseases, as well as many psychological disorders, rely on the analysis of *in vivo* measurements on the **cerebral cortex** using magnetic resonance imaging (MRI)."







CSR Challenges

Inter-subject variability

Partial Volume Effect

Limited MRI Resolution

Topology Defects

CorticalFlow

$$egin{aligned} & \mathrm{CF}^1_{ heta_1}(\mathbf{I},\mathcal{T}_1) = \mathrm{DMD}\Big(\mathrm{UNet}^1_{ heta_1}(\mathbf{I}),\mathcal{T}_1\Big) \ & \mathrm{CF}^{i+1}_{ heta_{i+1}}(\mathbf{I},\mathcal{T}_{i+1}) = \mathrm{DMD}\Big(\mathrm{UNet}^{i+1}_{ heta_{i+1}}(\mathbf{U}^\frown_1\cdots\mathbf{U}^\frown_i\mathbf{I}),\mathrm{CF}^i_{ heta_i}(\mathbf{I},\mathcal{T}_{i+1})\Big) \end{aligned}$$

Diffeomorphic Mesh Deformation (DMD)

Tractable framework for computing a diffeomorphic mapping Φ for each surface mesh vertex by solving the **flow ODE**,

$$rac{d\Phi(s;\mathbf{x})}{ds} = v\left(\Phi(s;\mathbf{x})
ight), ext{with } \Phi(0;\mathbf{x}) = x$$

using the iterative approximation method,

$$V^i_{k+1} = V^i_k + hv(V^i_k), ext{with} \;\; h = rac{1}{N}$$

provided by the forward Euler method.

- Retains the initial mesh topology without producing self-intersections.
- We also provide sufficient and comprehensible conditions for meeting the diffeomorphic properties of these transformations.

Related work: → Scaling & Squaring in DL Registration [1]: $\Phi^{(1/8)}=x+v/8$ $\Phi^{(1/4)} = \Phi^{(1/8)} \circ \Phi^{(1/8)}$ $\mathbf{\Phi}^{(1/2)} = \mathbf{\Phi}^{(1/4)} \circ \mathbf{\Phi}^{(1/4)}$ $\Phi^{(1)}=\Phi^{(1/2)}\circ\Phi^{(1/2)}$ **Voxel-wise integration** $|I| \gg |V|$ → Neural ODEs [2]: $\Phi(x)=x+\int_{0}^{1}f_{ heta}(x,I)dt$ vertex image feature extractor

[1] - Dalca, Adrian V., et al. "Unsupervised learning of probabilistic diffeomorphic registration for images and surfaces." *Medical image analysis* 57 (2019): 226-236.
 [2] - Gupta and Chandraker. "Neural mesh flow: 3d manifold mesh generation via diffeomorphic flows." *In Advances in Neural Information Processing Systems*, 2020.

Multiscale Training

Chamfer distance: Edge length regularizer: $\sum_{p\in V_p}\sum_{k\in \mathcal{N}(p)}||p-k||_2^2$ Pred Uniformly sample 150K points $-rac{1}{N} \left(\sum_{n \in P} \min_{s \in S} ||p-s||_2^2 + \sum_{s \in S} \min_{p \in P} ||p-s||_2^2 ight)$ $rgmin_{ heta_i} \sum_{(I,S)\in\mathcal{D}} \mathcal{L}\left(CF^i_{ heta_i}(I,\mathcal{T}_i),S ight)$ **Output Mesh**

CorticalFlow (CF³)

Experiments

- Dataset:
 - MRIs, Pseudo ground truth surfaces, and data splits proposed in [1].
 - 3876 MRI images from ADNI study
 - Pseudo ground truth surfaces generated with the **FreeSurfer V6.0 cross-sectional** pipeline.
 - Baselines:
 - QuickNAT [2]: Voxel-wise segmentation + surface extraction
 - Voxel2Mesh [3]: Deformable model with regularity penalties
 - NMF* [4]: Deformable model with diffeomorphic transformations
 - DeepCSR [1]: Implicit surface prediction + surface extraction + Topology Correction
 - Metrics:
 - Geometric accuracy: Chamfer distance, Hausdorff distance, and Chamfer normals.
 - Surface regularity: Percentage of self-intersecting faces using **PyMeshLab**.
 - Time and space complexity: Average inference time (in seconds) and inference GPU memory footprint (in GB) to reconstruct the **four cortical surfaces**.

- [3] Wickramasinghe et al. Voxel2mesh: 3d mesh model generation from volumetric data. In International Conference on Medical Image Computing and Computer-Assisted Intervention, 2020.
- [4] Gupta and Chandraker. Neural mesh flow: 3d manifold mesh generation via diffeomorphic flows. In Advances in Neural Information Processing Systems, 2020.

^{[1] -} Santa Cruz et al. DeepCSR: A 3d deep learning approach for cortical surface reconstruction. In Proceedings of the IEEE/CVF Winter Conference on Applications of Computer Vision, 2021.

^{[2] -} Roy et al. Quicknat: A fully convolutional network for quick and accurate segmentation of neuroanatomy. NeuroImage, 186:713–727, 2019.

Average Geometric Accuracy

Error color coded surfaces

Surface Regularity

QuickNAT Multiple connected components, handles and holes.

DeepCSR Anatomical mistakes due to topology correction

Surface Regularity

Inference Time and GPU Memory

Comparison to Pseudo-Ground-Truth

- → Orange circles highlight blurry MRI regions.
- → Green circles highlight FreeSurfer's underestimated area.
- → Red circles highlight non-plausible predictions avoided by CorticalFlow thanks to the diffeomorphism of its predicted deformations.

Future Applications

Segmentation at subvoxel resolution

QuickNAT inner surface segmentation

QuickNAT outer surface segmentation

CorticalFlow inner surface segmentation CorticalFlow outer surface segmentation

Analysis of surface descriptors on a common reference surface

Conclusion

This paper ...

- introduces CorticalFlow a novel geometric deep learning model for efficiently reconstructing <u>high-resolution</u>, accurate, and regular triangular meshes from volumetric images.
- derives a diffeomorphic mesh deformable (DMD) module that efficiently produces <u>diffeomorphic mappings</u> from stationary velocity field.
- shows that CorticalFlow is more accurate, robust, faster and memory efficient than state-of-the-art models in the cortical surface reconstruction problem which can facilitate <u>large-scale medical studies</u> and support <u>new healthcare applications</u>.

Australia's National Science Agency

CorticalFlow: A Diffeomorphic Mesh Transformer for Cortical Surface Reconstruction

https://lebrat.github.io/CorticalFlow/

